

AMENDMENTS TO THE SPECIFICATION

Paragraph [0002] of the specification is amended as follows:

In at least one known computed tomography (CT) imaging system configuration, an x-ray source projects a fan-shaped beam which is collimated to lie within an X-Y plane of a Cartesian coordinate system, wherein the X-Y plane is generally referred to as an "imaging plane". An array of radiation detectors, wherein each radiation detector includes a detector element, are within the CT system so as to ~~received~~ receive this fan-shaped beam. An object, such as a patient, is disposed within the imaging plane so as to be subjected to the x-ray beam wherein the x-ray beam passes through the object. As the x-ray beam passes through the object being imaged, the x-ray beam becomes attenuated before impinging upon the array of radiation detectors. The intensity of the attenuated beam radiation received at the detector array is responsive to the attenuation of the x-ray beam by the object, wherein each detector element produces a separate electrical signal responsive to the beam attenuation at the detector element location. These electrical signals are referred to as x-ray attenuation measurements.

Paragraph [0035] of the specification is amended as follows:

Moreover, the noise value of the original image σ_o may also be estimated by equating σ_o with the noise pattern of the selected phantom image wherein adjustments have been made to compensate for differences between the scanning technique used to obtain the original image and the scanning technique and processing used to obtain the selected phantom image. In addition, σ_o may be determined by summing the pixel data in the vertical and horizontal orientations and subsequently using a noise prediction strategy as described in U.S. Application serial No. 10/064,874, ~~Attorney Docket No. 122942~~ U.S. Patent Publication No. 2004-0032928A1.